

## STUDY OF NOVEL GEOMETRIES FOR OSCILLATORY BIMORPH ACTUATOR OF A PIEZOELECTRIC FLOW PUMP

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**Abstract.** Nowadays, precision flow pumps are instruments widely applied through many Engineering areas, such as cooling of electronic components and Bioengineering applications for fluid pumping through an organism. New principles in precision flow pumps development have been extensively proposed, such as the one based on the use of piezoelectric actuators. A piezoelectric flow pump presents some advantages in relation to other solutions, such as miniaturization potential, and fewer numbers of moving parts, and it also offers better performance with low noise and low power consumption. This work presents the development of novel configurations of piezoelectric flow pumps based on the use of oscillatory bimorph actuators with biomimetic tip geometries that are inspired in fish caudal fin shapes. The flow generation principle, based on vortices generated by oscillation of the piezoelectric actuators, is analogous to the fish swimming tail during its locomotion. This flow pump development consists in computational simulations, manufacturing and experimental characterization steps. The main objective is to analyze the efficiency of the proposed shapes of bimorph piezoelectric actuators in fluid pumping. The experimental methodology and obtained results are presented, as well as, a way of analyzing the physical phenomena and validating these new proposed designs.

**Keywords:** oscillatory pump, piezoelectric actuator, experimental characterization, computational simulation.

### 1. INTRODUCTION

Precision flow pumps have been studied over the last decades. It has small size, low power consumption, and it can be applied as an essential component for drugs and chemical reagents dosage systems (Tsai and Sue, 2007), and for pumping systems of biological fluids (Andrade et al., 1996), and for cooling systems of electronic equipment. Traditional cooling systems (using fans) became inefficient to dissipate the heat generated by the modern chips. In order to solve these technological problems, use of water cooling systems, based on precision flow pumps and small heat exchangers, having higher thermal dissipation capacity, have been proposed by many researchers (Singhal et al., 2004).

Several works use piezoelectric actuators in precision flow pumps since it presents some advantages in relation to other solutions, such as miniaturization potential, lower noise generation, and fewer numbers of moving parts (Kim et al., 2004). Bar-Cohen and Chang (2001) presents an ultrasonic pump which uses stators piezoelectrically actuated to generate a propagating wave that moves the fluid. This kind of flow pump has also been developed by other researches (Smits, 1990; Teymoori and Abbaspour-Sani, 2005; Jang and Kan, 2007). Other example is a diaphragm pump, in which the piezoelectric actuator works as a membrane, which it forces fluid through a small chamber, having the flow direction controlled by check valves (Meng et al., 2000). Another example of piezoelectric pump has been studied by Kar et al. (1998), which is based on a mechanism similar to a syringe that uses a piezoelectric actuator to control its dosage.

Lima et al. (2009) presents the principle of a novel pump configuration based on placing a rectangular oscillating bimorph piezoelectric actuator in a fluid channel to generate flow. The proposed principle of pumping mimics a phenomenon of the swimming fish (Sfakiotakis et al., 1999), through an oscillatory motion generated by a thin plate oscillating inside a fluid environment. This oscillatory behavior yields vortex interaction that result in a flow rate due to the action and reaction principle.

Investigation of vibration modes, in what such phenomena occurs, gives motivation for the exploration of new shapes for the bimorph piezoelectric actuator. Thus, the objective of this present work is the development of novel configurations of piezoelectric flow pumps based on the use of bimorph actuators with biomimetic tip geometries that are inspired in fish caudal fin shapes in order to explore the novel pump principle proposed by Lima et al. (2009), aiming to maximize the pump performance.

In the next sections, the complete cycle of pump development is shown. Initially, section 2 presents the fundamental theory. In section 3, proposed tail shapes are described. Section 4 shows analysis of proposed tail shapes from computational simulations. Section 5 describes the applied experimental apparatus and results achieved using manufactured prototype pump. Finally, some conclusion is given in Section 6 about obtained results.

## 2. FUNDAMENTAL THEORY

The wake generated by fish that swims due to undulatory and/or oscillatory motion of their bodies and caudal fins is a discrete vortex street of alternating sign, as it can be seen in Fig. 1. This vortex street has reversed rotational direction compared to the Karman vortex street, which produces drag force around bodies placed in a free stream (Sfakiotakis et al., 1999), and then, flow generation between the vortices can be observed.

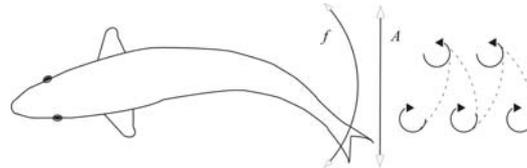


Figure 1. Vortex street wake generated by a fish swimming

Similar vortex street generation is also observed in oscillatory motion of a thin plate inside a fluid environment (Açikalin et al., 2003). In this way, each generated vortex drives the one generated previously in opposite direction to the actuator (thin plate), resulting in a flow rate to the right side due to the action and reaction principle. Lima et al. (2009) explores this working principle by applying it to a novel pump configuration based on oscillating bimorph piezoelectric actuator placed in a fluid channel to generate flow, as illustrated in Fig. 2.

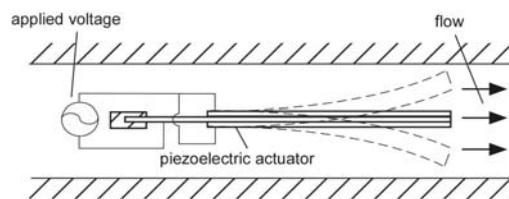


Figure 2. Piezoelectric pump scheme

In this work, the influence of using bimorph piezoelectric actuators with different tail shape is investigated. A bimorph piezoelectric actuator is an electromechanical flexible actuator mounted as a clamped beam with a free end. Its construction consists of a metallic plate allocated between two piezoelectric ceramic layers. When an electric voltage is applied to the ceramic, the metallic plate is deformed proportionally to the applied voltage, as illustrated in Fig. 2. Combination of a bimorph (PZT/metal/PZT) allows such displacements since when a piezoelectric ceramic is expanded the other is compressed, bending the actuator. A bimorph actuator shows relative high displacements ( $\sim 1$  mm), however with very low forces. Operating in resonant frequency its typical response is achieved around  $50 \mu\text{m}/\text{V}$ .

## 3. PROPOSED SHAPES

Different fish tail shapes shown in Fig. 3 are reproduced on metal thin plates, which are assembled at the free end of the bimorph piezoelectric actuator. These tail shapes were also studied by Wiguna et al. (2005) to analyze its influence in fish robot propulsion. Vibration modes of each piezoelectric actuator configuration, with thin plate attached, are calculated and its effect in vortex generation at pumping flow is investigated.

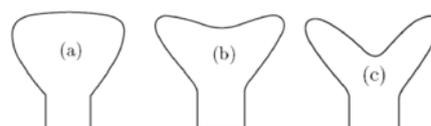


Figure 3. Fish tail shapes: a) ostraciiform; b) subcarangiform; c) carangiform

The first proposed shape is based on fish tail ostraciiform shape (Fig. 3a) which has a triangular geometry with small elongation in central region. Other configuration, based on fish tail subcarangiform shape (Fig. 3b), has a triangular geometry with small concavity in central region. This concavity generates a narrow tail tip region, which reduces the

stiffness of this region, yielding a high amplitude oscillatory tip. Another study is made considering configuration based on fish tail carangiform shape (Fig. 3c) which has a large concavity in central region. Fish having tail carangiform shape uses 1/3 of its body for oscillatory propulsion, while the fish having tail subcarangiform shape uses a large fraction of its body (1/2 up to 2/3) for locomotion (Sfakiotakis et al., 1999).

Computational simulations, using finite element analysis (FEA), are carried out for piezoelectric actuators with attached thin plates that mimic fish tail shapes presented in this section. After that, experimental prototype characterization is made to investigate flow rate generated from each one.

#### 4. COMPUTATIONAL SIMULATIONS

The use of computational models allows the evaluation of a given system behavior reducing the prototype construction costs. Thus, computational models of bimorph piezoelectric actuator configurations (see Fig. 4) are simulated through an acoustic harmonic analysis, in which the system resonant frequencies and vibration modes both in air and in liquid environment are identified.

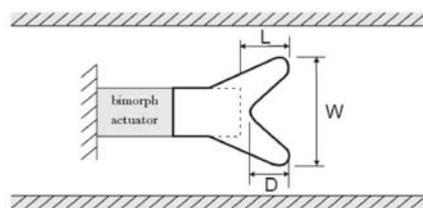


Figure 4. Parametric model for acoustic analysis

In this work, the piezoelectric pump simulation is performed by using the ANSYS finite element software, however any other appropriate FEA tool could also be used. An acoustic model of the pump water channel is created by using FLUID30 element (Ansys, 2003) to simulate fluid-structure interaction. Inside the channel, the bimorph piezoelectric actuator is modeled by using SOLID98 element that allows performing tridimensional simulations of structural materials, such as copper and piezoelectric materials.

Figure 5 shows a section view of the FE mesh (with tetrahedral elements) used in computational simulations. An intermediate region (red layer in Fig. 5) between solid region (piezoelectric actuator and duct walls) and fluid medium (water) is needed to provide fluid-structure phenomena.

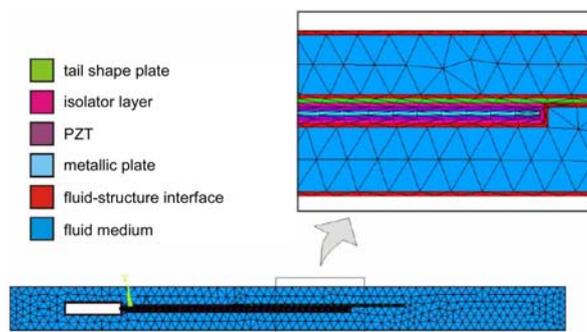


Figure 5. Section view of FE mesh used in simulations

The fluid medium adopted in this work is water, and the boundary conditions of pump channel model used in the acoustic analysis consists of applied voltage values for electrode regions (equal to 30V at PZT element and 0V at metallic plate element), and null displacement values for region near the piezoelectric actuator clamp.

Convergence analysis is performed to determine the influence of the mesh discretization in simulations. According to computational simulations, the FE mesh composed by 200,000 elements (approximately) is chosen since frequency and amplitude convergence is found for this discretization. Moreover, it is noticed that for larger refined mesh the computational cost is very high.

The vibration modes and the frequency spectrum are obtained for the same geometric parametric model shown in Fig. 4, using the following adopted parameter:  $W=40$  mm;  $L=20$  mm; and  $D=10$  mm. Figure 6 presents the third vibration modes of the system composed by piezoelectric actuator and thin plate. In this work, the third vibration mode is chosen for all computational models since this mode is a variation of the actuator second mode, which is characterized by a peak formation in the middle of the actuator. From Fig. 6, it is noticed that thin plate tip behavior presents higher displacements, whose probable effect is to provide higher fluid flow generation.

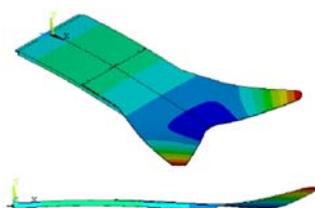


Figure 6. Third vibration mode

Here, obtained frequency values are related to the piezoelectric actuator impedance values near its resonant frequency. The experiments are conducted in the resonant frequency because the maximum electromechanical conversion of material occurs in this frequency, which results in large displacements.

A sensitivity analysis is also performed. Essentially, it consists of changing some parameters values (W, L, and D of parametric model shown in Fig. 4 to verify the influence of each one in the obtained results. Several different possible combinations of these parameters are also tried out in order to find better performance of the system composed by piezoelectric actuator and thin plate. The model used in convergence analysis (W=40, L=20, D=10) is chosen as reference model for comparison using the results obtained in the sensitivity analysis. As selection criteria, the chosen combination should give high amplitude together with high frequencies for maximizing piezoelectric pump performance. Thus, the best simulation results are obtained for parameter combinations shown in Tab. 1.

Table 1. Computational results obtained in acoustic simulations

W (mm)	L (mm)	D (mm)	F (Hz)	Displacement (mm)
40	20	10	<b>369.0</b>	<b>1.412</b>
30	20	10	<b>412.0</b>	<b>1.361</b>
30	15	10	<b>529.0</b>	<b>1.532</b>
40	15	10	<b>446.5</b>	<b>1.504</b>
40	20	0.5	<b>358.0</b>	<b>1.377</b>
40	20	5	<b>358.0</b>	<b>1.590</b>

The displacement of the piezoelectric actuator model found in this harmonic analysis could be prescribed as boundary condition in a fluid flow simulation to reproduce the behavior of the flow pump. However, a fluid analysis requires high computational time making unfeasible to drive simulation of a high number of parametric model combinations. Due to this, experimental approach is adopted to verify flow rate levels of the best models studied in acoustic analysis (W, L, D combinations shown in Tab. 1).

## 5. EXPERIMENTAL RESULTS

### 5.1. Experimental Apparatus

The experimental apparatus utilized in this work is designed to allow making changes in the pump channel geometry quickly. Figure 7 illustrates this apparatus.



Figure 7. Experimental apparatus

The experimental characterization results consist of obtaining electrical impedance curves for each piezoelectric actuator and the respective flow rate values. The electrical impedance curves for a frequency range are obtained by using a HEWLETT PACKARD 4194A impedance analyzer. The frequency range adopted varies from 100Hz (minimum frequency of the instrument) to 1200Hz.

The pump flow rate measurement is made by measuring the maximum flow velocity inside a cylindrical tube, made of acrylic material. This tube has 12.7 mm diameter and 75 mm length, and it is placed inside a channel where the water flows (see Fig. 7). By measuring the time that the liquid (water) takes to cross the known tube length, the flow rate can be calculated (Fox and McDonald, 1998). Thus, based on the continuity principle, it is concluded that flow rate generated by the flow pump inside the channel is the same as the one calculated inside the tube. To facilitate the time measurement a red pigment is used in the water, allowing to visualize the fluid flow inside the system.

## 5.2. Results

A prototype of each piezoelectric actuator configuration (with attached thin plate), which respective model provides the best results in computational simulations (see W, L, D combinations shown in Tab. 1), is constructed and its corresponding electrical impedance curves are determined in air and water. Through these obtained electrical impedance curves it is possible to determine the resonant frequencies for each prototype and, consequently, probable excitation frequencies that produce higher flow rate. The values obtained in this electrical impedance analysis provide data input for the flow rate experimental tests shown in this section.

Figure 8 illustrates apparatus configurations considered for experimental flow rate measurement. Three different channel width values (60, 80, and 100 mm) are tested. In this case, the influence of these dimension parameters in flow rate measurement is verified.

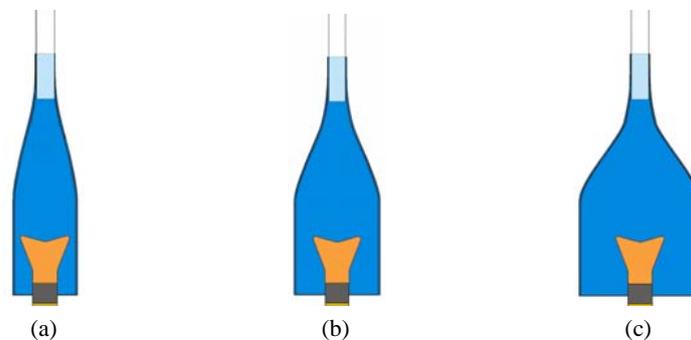


Figure 8. Pump channels tested. (a) width = 60 mm; (b) width = 80 mm; (c) width = 100 mm

The flow rate measurement is carried out for all constructed piezoelectric actuator configuration, however the best results is obtained for prototype with thin plate parameters equal to  $W=40$  mm,  $L=20$  mm, and  $D=0.5$  mm. The flow rate values obtained considering the tested pump channels (see Fig. 8) are 114 ml/min, 95 ml/min, and 85 ml/min, respectively (60 mm, 80 mm, and 100 mm of channel width). The obtained results correspond to frequencies in which the pump presented the best performance in terms of flow rate.

The reference flow rate value in channel of Fig. 8a is 81.4 ml/min (at 414 Hz), achieved by using a rectangular piezoelectric actuator, which has 40 mm length, 20 mm width, and 0.6 mm thickness, without attached thin plate.

## 6. CONCLUSION

Computational simulations are performed to determine resonant frequencies and respective vibration modes of the novel configurations of bimorph piezoelectric actuator. Through this development, it is possible to find parameters that have considerably influence in flow pump performance. According to obtained results, the channel dimensions have influence in generated flow rate values. It is concluded that using of biomimetic thin plates on bimorph piezoelectric actuators for applications in fluid pumping provides good effects in the performance of oscillatory piezoelectric flow pumps. It is possible to see that in some cases the application of biomimetic thin plates on the piezoelectric actuator gives higher flow rate, achieving an improvement of 40% in terms of flow rate, in relation to the bimorph piezoelectric actuator with traditional rectangular shape.

As suggestions for future work, a more complete analysis of the influence of channel profile in the performance of oscillatory piezoelectric flow pumps will be conducted through fluidic simulations, contributing to improve the knowledge about the involved phenomena. Finally, a study about this system miniaturization to obtain a more compact apparatus is also suggested.

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## 8. REFERENCES

- Acikalin, T., Raman, A., and Garimella, S. V., 2003, "Two-dimensional streaming flows induced by resonating, thin beams", *J. Acoustical Society of America*, 114(4), pp. 1785–1795.
- Andrade, A. J. P., et al., 1996, "Characteristics of a blood pump combining the centrifugal and axial pumping principles: The spiral pump", *Artificial Organs*, 20, pp. 605–612.
- Ansys, Inc., 2003, "Theory Reference: Fluid Flow".
- Bar-Cohen, Y. and Chang, Z., 2001, "Piezoelectrically actuated miniature peristaltic pump", in *Proceedings of SPIE's 8th annual International Symposium on Smart Structures and Materials*.
- Fox, R. W. and McDonald, A. T., 1998, "Introduction to Fluid Mechanics", John Wiley & Sons, New York.
- Jang, L. S. and Kan, W. H., 2007, "Peristaltic piezoelectric micropump system for biomedical applications", *Biomedical Microdevices*, 9, pp. 619–626.
- Kar, S., McWhorter, S., Ford, S., and Soper, S., 1998, "Piezoelectric mechanical pump with nanoliter per minute pulse-free flow delivery for pressure pumping in micro-channels", *Analyst*, 123(7), pp. 1435–1441.
- Kim, Y., Wereley, S., and Chun, C., 2004, "Phase-resolved flow field produced by a vibrating cantilever plate between two endplates", *Physics of fluids*, 16(1), pp. 145–162.
- Lima, C. R., Vatanabe, S. L., Choi, A., Nakasone, P. H., Pires, R. F., and Silva, E. C. N., 2009, "A biomimetic piezoelectric pump: Computational and experimental characterization", *Sensors and Actuators: A-Physical*, DOI: 10.1016/j.sna.2009.02.038.
- Meng, E., et al., 2000, "A check-valved silicone diaphragm pump", *Proceedings IEEE Micro Electro Mechanical Systems*, Miyazaki, Japan, pp. 6267.
- Sfakiotakis, M., Lane, D., and Davies, B., 1999, "Review of fish swimming modes for aquatic locomotion", *Journal of Oceanic Engineering*, 24(2), pp. 237–252.
- Singhal, V., Garimella, S. V., and Raman, A., 2004, "Microscale pumping technologies for microchannel cooling systems", *Applied Mechanics Reviews*, 57, pp. 191–221.
- Smits, J. G., 1990, "Piezoelectric micropump with three valves working peristaltically", *Sensors and Actuators A-Physical*, 21-23, pp. 203–206.
- Teymoori, M. M. and Abbaspour-Sani, E., 2005, "Design and simulation of a novel electrostatic peristaltic micromachined pump for drug delivery applications", *Sensors and Actuators A-Physical*, 117(2), pp. 222–229.
- Tsai, N.-C. and Sue, C.-Y., 2007, "Review of mems-based drug delivery and dosing systems", *Sensors and Actuators: A-Physical*, 134, pp. 555–564.
- Wiguna, T., Syaifuddin, M., Park, H. C., and Heo, S., 2005, "Mechanical design, fabrication and test of biomimetic fish robot using LIPCA as artificial muscle", *Dept of Advanced Techn. Fusion, Konkuk University, Seoul, Coria do Sul*.

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